Convolutional Reccurent Neural Networks for Electrocardiogram Classification

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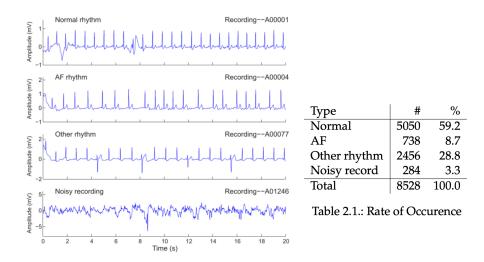
CRNN for ECG

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Problem



- Atrial fibrillation (AF) occurs in 1-2% of population
- Associated with significant mortality and morbidity
- Existing AF detection methods are not precise and require special multi-lead equipment
- It is proposed to use a single-lead ECG and leverage data processing techniques to be on par with multi-lead detectors
- Challenge limited data + strict inference requirements

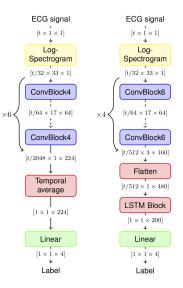


Network architectures

- 24-layer CNN
- CRNN that combines a 24-layer CNN with a 3-layer LSTM network.

Both architectures consist of four parts:

- data preprocessing with log-spectrogram
- stack of convolutional layers for feature extraction
- aggregation of features across time by averaging and LSTM block in case of CNN and CRNN, respectively
- Iinear layer with Softmax classifier



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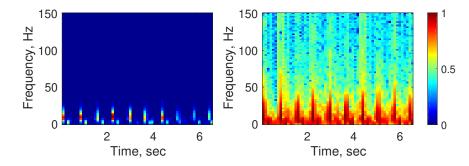
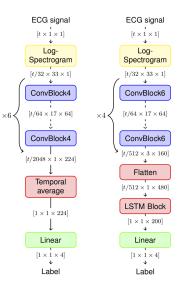


Figure: Normalized spectrogram (left) and normalized logarithmic spectrogram (right) of an example ECG signal.

Convolutional layers

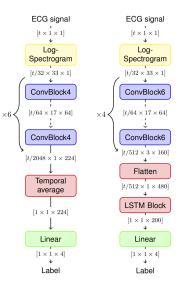
- 5×5 filters, ReLU activation
- grouped in blocks of 4 and 6 layers for CNN and CRNN, respectively
- number of channels is constant inside blocks, last layer in block applies max-pooling over 2 × 2 windows and increases number of channels
- number of channels after first block is 64 and increased by 32 by each subsequent block



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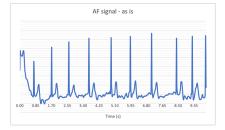
Feature aggregation across time

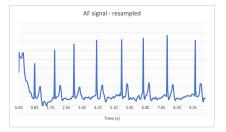
- ConvBlocks produce variable length outputs, need to be aggregated across time to be fed into classifier.
- CNN aggregation via simple averaging. Temporal smoothing of features, not suited to classify episodic phenomena occurring only during a short time span.
- CRNN aggregation via 3 layer LSTM with 200 neurons in each layer. Aggregation of features in a highly non-linear manner across time, potentially better preservation of episodic phenomena.



We employ two data augmentation techniques, namely *dropout bursts* and *random resampling*.

- Dropout bursts selecting time instants uniformly at random and setting the ECG signal values in a 50ms vicinity of those time instants to 0. Dropout burst hence model short periods of weak signal due to, e.g., bad contact of ECG leads.
- Random resampling assuming a heart rate of 80bpm, uniformly resamples the ECG signals such that the heart rate of the resampled signal would be uniformly distributed on the interval [60, 120]bpm. Random resampling thus emulates a broader range of heart rates.





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Results (estimated using 5-fold cross validation)

Arch.	metric	Ν	А	0	~	overall
CNN	acc.	88.1	83.6	66.9	77.1	81.2
	F_1	87.8	79.0	70.1	65.3	79.0
CRNN	acc.	89.9	77.8	69.4	71.5	82.3
	F_1	88.8	76.4	72.6	64.5	79.2

Table: Accuracies (acc.) and F_1 scores (in %) for the proposed network architectures.

Arch.	metric	Ν	А	0	~	overall
CNN	acc.	90.5	64.2	68.0	54.9	80.5
	F_1	88.3	69.9	69.1	59.6	75.8
CRNN	acc.	90.2	69.1	63.0	51.1	79.2
	F_1	87.4	69.9	66.5	54.9	74.6

Table: Accuracies (acc.) and F_1 scores (in %) for the proposed network architectures with *data augmentation deactivated*.

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Ensemble of 5 CRNN networks.

- Partitioning into 5 equally sized subsets, 4 for training and 1 for validation/early stopping.
- Each network in the ensemble uses a different validation subset. Therefore, all available data was used in training.
- The size of submission is 273.9mb, the ensemble on average consumed 58.1% of computational quota available.

- Results show that aggregation of features with LSTM is more effective than averaging. However CRNN has more parameters and thereby higher model capacity.
- The data augmentation proved to be effective, thus indicating that it captures certain real world phenomena.
- Tried to pretrain the CNN and the convolutional layers of the CRNN on the PTB Diagnostic ECG Database [Bousseljot et al., 1995]. Did not lead to improvements.
- Possible improvement extending the data augmentation scheme, e.g., by taking the actual heart rate into account for random resampling (instead of assuming 80bpm).

- [Cakır et al., 2017] CRNN for polyphonic sound detection. Input signal is mapped to the sequence of labels.
- [Bashivan et al., 2016] CRNN for mental state classification from electroencephalogram (EEG) data.
- [Lipton et al., 2016] LSTM networks are used for multilabel classification of diagnoses in electronic health recordings.
- [Rajpurkar et al., 2017] deep CNN architecture for arrhythmia detection in ECGs, but unlike in the classification problem considered here, maps the ECG signal to a sequence of rhythm classes.

References I

Bashivan, P., Rish, I., Yeasin, M., and Codella, N. (2016). Learning representations from EEG with deep recurrent-convolutional neural networks.

In Proc. Int. Conf. on Learn. Representations (ICLR).

Bousseljot, R., Kreiseler, D., and Schnabel, A. (1995). Nutzung der EKG-Signaldatenbank CARDIODAT der PTB über das Internet.

Biomedizinische Technik/Biomedical Engineering, 40(s1):317–318.

Cakır, E., Parascandolo, G., Heittola, T., Huttunen, H., and Virtanen, T. (2017).

Convolutional recurrent neural networks for polyphonic sound event detection.

IEEE/ACM Trans. on Audio, Speech, and Language Processing, 25(6):1291–1303.

- Lipton, Z. C., Kale, D. C., Elkan, C., and Wetzell, R. (2016). Learning to diagnose with LSTM recurrent neural networks. In *Proc. Int. Conf. on Learn. Representations (ICLR).*
- Rajpurkar, P., Hannun, A. Y., Haghpanahi, M., Bourn, C., and Ng, A. Y. (2017).

Cardiologist-level arrhythmia detection with convolutional neural networks.

arXiv preprint arXiv:1707.01836.